

SYNTHESIS AND APPLICATION OF CHITOSAN HYDROXYAPATITE: A REVIEW

Noira R. Vokhidova^{a, *}, Kandiyor H. Ergashev,
Sayyora Sh. Rashidova

*Institute of Polymer Chemistry and Physics, Uzbekistan Academy of Sciences, Tashkent,
100128, Uzbekistan*

^a - ORCID: 0000-0003-0477-3708

** corresponding author: noira_vokhidova@yahoo.de*

Abstract

In this review, the research devoted to synthesising chitosan apatites, their biologically active properties, and their application in medical practice is analysed. The data are from articles published between 2001 and 2022 on the formation of calcium- and phosphorus-containing chitosan composites and the mechanism of their interaction.

Keywords: *chitosan, Bombyx mori, polymer, hydroxyapatite, composite, nanostructure, bone, osteoporosis, traumatology, orthopaedics, dentistry*

Received: 06.02.2022

Accepted: 18.05.2022



1. Introduction

Safe, non-toxic bio-preparations based on chitosan (ChS) and its derivatives are widely used in medical and veterinary practice. Calcium and phosphorus are biologically important elements that form the support systems of living organisms. Their deficiency contributes to the weakening of the bone system, the tendency to develop fractures and cracks, osteoporosis, tooth decay, changes in appetite and weight, numbness, stunted growth and development. Currently, diseases arising from calcium and phosphorus deficiencies, particularly osteoporosis, are included in the list of economically significant diseases.

With increasing life expectancy worldwide, the number of older people in each geographic region is increasing, and the incidence of fractures in 2050 is expected to reach 6.26 million [1]. Hence, the need for calcium- and phosphorus-containing drugs is increasing year by year. According to 2010 data, osteoporosis affected 200 million women and 120 million men worldwide, and the proportion increases with age. The disease affects 1 in 3 women and 1 in 5 men over the age of 50 years [2]. It is critical to study the fundamentals of obtaining composites of ChS and hydroxyapatite (HA), the features of their interaction, establishing the chemical composition and structure, and their properties. The creation of polymer-apatite drugs needed to support calcium and phosphorus balance is of great interest. These preparations are import substituting and can be used to improve the efficiency of egg-laying hens as well as to prevent and treat osteomalacia and osteoporosis. This review systematises and analyses the most important research results on the production of ChS apatites and their application in traumatology, orthopaedics, and dentistry.

2. Features of the Chemical Interactions of ChS

Chitin (ChT) is a linear amino polysaccharide composed of *N*-acetyl-2-amino-2-deoxy-*D*-glucopyranose units acting as the outer skeleton and support of the cuticle of crustaceans and insects. As a soluble derivative of ChT, ChS is a copolymer of *D*-glucosamine and *N*-acetyl-*D*-glucosamine. ChT and ChS are biologically active polymers [3, 4]. Depending on the conditions of the reaction, the degree of deacetylation (DD) of ChS can reach up to 95%. The DD cannot reach 100% because the acetamide groups are in the transposition and complete substitution of acetamide groups is impossible (Figure 1).

ChS is a rigid-chain polymer and a compositionally heterogeneous polysaccharide. It is characterised by molecular polydispersity, pH-dependent solubility, and a tendency to form hydrogen bonds. These abilities underlie its uniqueness and unpredictability. The deprotonated amino groups in ChS interact with *d*-metal ions to form chelates and metal complexes [5, 6]. The presence of electron-donating functional groups in ChS promotes the formation of intra- and intermolecular hydrogen bonds. This allows ChS to bind to organic compounds, including toxins.

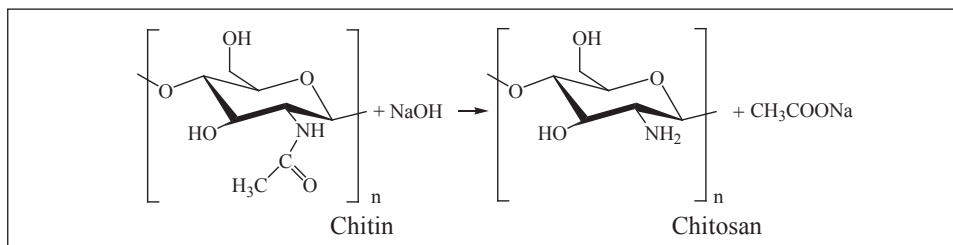
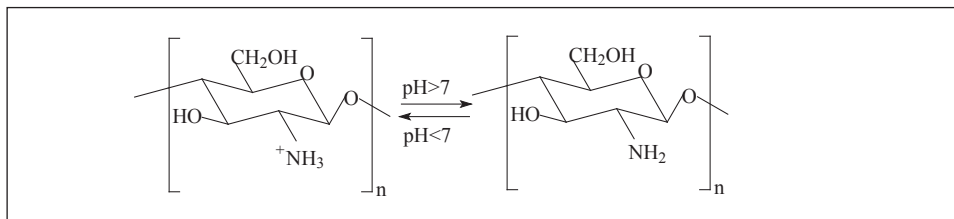


Figure 1. The reaction that produces chitosan from chitin.

The presence of hydrogen bonds reduces the solubility of ChS because the ChS-ChS hydrogen bonds are stronger than the ChS-solvent hydrogen bonds. ChS swells and dissolves in an acidic medium – that is, in organic and mineral acids (vinegar, oxalate, lemon, amber, hydrochloric acid, etc.). The reactivity and physicochemical properties of ChS are directly related to will pH of the medium:



In an acidic medium, the amino groups of ChS are protonated. At pH 6.5, phase separation occurs and ChS precipitates [5].

ChS is chemoselective: deprotonated amino groups, as well as hydroxyl (-OH) groups on carbons C3 and C6, allow ChS to undergo nucleophilic substitution (S_N) and addition (A_N). It should be noted that by varying the synthesis conditions, it is possible to obtain *N*- and *O*-derivatives of ChS owing to the presence amine (- NH_2) and -OH groups (Figure 2).

ChS possesses unique physicochemical and biological properties, among which its biocompatibility, antimicrobial effect, and immunomodulatory properties, can be distinguished. ChS is also an antiviral, fungicidal, bioavailable, hypoallergenic, and harmless natural polymer that promotes tissue regeneration [7-9]. The ability to use ChS obtained from various sources is determined by a unique combination of several physicochemical and biological properties:

- high reactivity;
- biocompatibility;

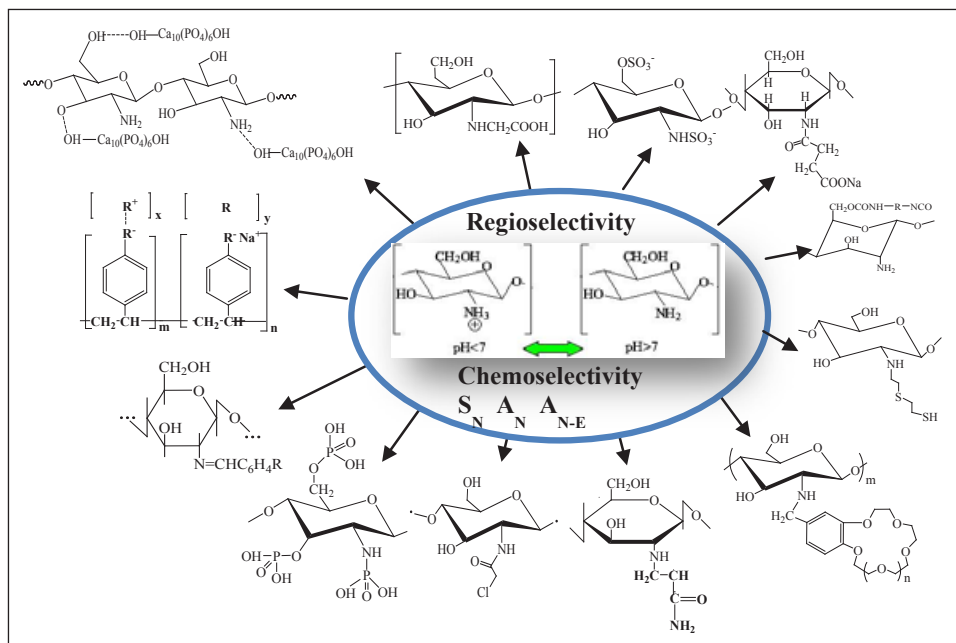


Figure 2. Possible chemical reactions in chitosan chains.

- biodegradability;
- bacteriostatic activity;
- immune-stimulating activity; and
- selectivity, with excellent adsorption capacity of aqueous solutions, solvents, and especially heavy metals.

ChS is used in dentistry to treat conditions such as gingivitis and periodontitis because it rebuilds the connective muscle tissue that covers the gums. ChS is also used as an artificial skin substitute and has been found to have no side effects after tissue implantation [10].

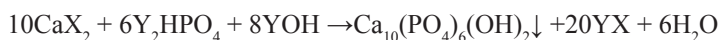
The role of functional biomaterials in tissue engineering in medicine and veterinary medicine is invaluable. Biomaterials must meet a number of requirements, in particular, maintain the shape and dimensions of tissues, be biodegradable and hypoallergenic, have minimal side effects, and have a mechanically strong porous structure that stimulates tissue growth [9]. ChS possesses these properties: its biodegradation, bioavailability, and bioactive properties make it an effective biopolymer that can be used in tissue engineering, including the regeneration of skin, bones, liver, nerves, and muscles [11-16].

Due to its unique properties, ChS is used in more than 80 branches of the economy. One of the advantages of ChS is its renewability, unlimitedness, and variety of sources for its production. ChS is isolated from carapaces, fungi, dead bees, and other sources [17]. There has also been great interest and investigation of the various derivatives and modifications of ChS obtained from *Bombyx mori*.

3. Synthesis and Properties of Calcium HA

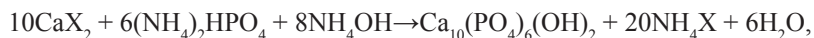
HA – with the chemical formula $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ – differs from other calcium phosphates by isomorphism, thermal and chemical stability, composition stoichiometry, and structural properties similar to the skeletons of humans and living organisms [18]. There are several different methods to synthesise HA [19-22], including (1) liquid phase synthesis (wet method), (2) solid-phase synthesis (dry method), (3) hydrothermal synthesis, (4) sol-gel, and (5) hydrolysis.

Highly dispersed powdered HA is usually obtained by a two-way exchange reaction as follows (liquid-phase synthesis):



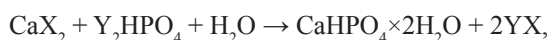
where $\text{X} = \text{NO}_3^-$, Cl^- , or CH_3COO^- and $\text{Y} = \text{NH}_4^+$, K^+ , or Na^+

The interaction between any calcium and phosphate (PO_4^{3-}) salts and the composition of the target reaction product depend on the pH, duration of synthesis, temperature, and the calcium-to-phosphorus (Ca/P) molar ratio in solution. The formation of HA occurs at relatively low temperatures or within a few seconds during long-term recrystallisation of amorphous calcium phosphate (AKP) at $>50^\circ\text{C}$. Usually, nonstoichiometric HA is formed, namely $\text{Ca}_{10-x}(\text{HPO}_4)_x(\text{PO}_4)_{6-x}(\text{OH})_{2-x}$, where x depends on the synthesis conditions [23, 24]. For example, for the synthesis of HA gel, aqueous solutions of ammonium hydrogen phosphate with calcium salts are stored under strong conditions for 10 days in a highly alkaline medium (pH 10-11) and washed with distilled water to pH 7.0-7.2 [25]:



where $\text{X} = \text{Cl}^-$ or NO_3^- . If the synthesis is carried out according to the above scheme at pH 4-5, a mixture of monoclinic syngonite brushite ($\text{CaHPO}_4 \cdot 2\text{H}_2\text{O}$) or brushite and triclinic-syngonite monetite (CaHPO_4) can be obtained:





where X = NO₃⁻, Cl⁻, or CH₃COO⁻ and Y = NH₄⁺, K⁺, or Na⁺ (at 70-90°C) [26].

HA has been obtained from calcium nitrate and ammonium hydrogen phosphate in an aqueous solution at Ca/P ratios of 1.31 and 1.64, respectively, after a 48-h reaction [27]. The authors compared the physicochemical properties of these samples with HA obtained at a Ca/P ratio of 1.56. X-ray diffraction analysis showed the presence of phases corresponding to HA and β-calcium phosphate.

In the synthesis of HA, it is important to pay attention to its crystalline and amorphous structure. The first solid phase, formed upon rapid stirring of aqueous solutions of salts containing Ca²⁺ and PO₄³⁻, consists of AKP. They are thermodynamically unstable compounds that, if not stored under dry conditions or with the addition of a stabiliser, transform spontaneously into crystalline calcium orthophosphate (CaPO₄) – that is, calcium apatites [28]. One of the special properties of calcium apatites is their solubility in acidic media. Describing the degree of dissociation, chemical changes occur with all ions during diffusion through the Nernst layer. The chemical composition of the apatite surface during melting, sorption, and decomposition; the initial stages of porosity; ion sorption; surface diffusion; and specific effects during decomposition are critical factors [29]. In addition to materials based on HA, regenerative or fully absorbable materials have been elaborated. They are based on the use of a porous resorbed matrix that carry proteins and bone cells for tissue engineering.

Calcium phosphate-based materials such as HA, tricalcium phosphate (TKP, Ca₃(PO₄)₂), and carbonate-substituted carbonate-hydroxyapatite (KHA) possess effective biological properties, high protein adsorption, good osteoclast function and osteoblast formation in tissues, and participation in bone regeneration [30].

Researchers have created HA composites that closely resemble bone tissue. These composites comprise polymers such as ChS, collagen (Col), and gelatine (G). As a result, some of the ceramic properties of HA, such as its intrinsic fragility, the structure, and migration of particles from their places of residence, can be ameliorated. Studies suggest that biocomposites for biologically active and biodegradable artificial bones and bone deficiency [31]. The main component of bone tissue (>75%) is calcium, and carbonate accounts for about 4% [32-34] up to 7% [35].

When evaluating natural and synthetic apatites, there is intense assimilation of PO₄³⁻ according to Fourier-transform infrared (FTIR) spectroscopy. The carbonate groups that make up KHA are located on a hexagonal axis that holds the -OH (A-type exchange) or PO₄³⁻ (B-type exchange) groups. This tissue is characterised by the presence of mixed AB types [36, 37].

The nature of calcium phosphates is diverse. Their Ca/P molar ratio is about 1.67. It was found that at the ratio Ca/P > 1.67, when interacting with water, a strongly alkaline medium is obtained. And at Ca/P < 1.67, it leads to the formation of insoluble and unstable composites when interacting with water or physiological fluids [38]. Calcium phosphates at a Ca/P ratio of < 1.67 include TKP, calcium pyrophosphate (CPP, Ca₂P₂O₇), calcium polyphosphate ((Ca(PO₃)₂))_n, and KHA (Na₂O-CaO-P₂O₅, Na₂O-CaO-P₂O₅-SiO₂, K₂O-CaO-P₂O₅) [39]. Metal-HA has been synthesised by replacing calcium in HA with metals such as zinc (Zn), copper (Cu), and magnesium (Mg). The authors found more effective biological activity for Ca_{10-x-z}(Me_z(HPO₄)_y(PO₄)_{1-y/6}(OH)₂) and Ca_{10-x-z}(Cu_z(HPO₄)_y(PO₄)_{1-y/6}(OH)₂) containing 1% Cu [40]. Ag Ca_(10-x)Ag_x(PO₄)₆(OH)_(2-x), = 0.3 (Ag-HA, Ca/P=1.616) have also been synthesised. It possesses antibacterial properties when applied at the implant surface. The molecule has a Ca/P ratio of 2.25 ± 0.25 and a (Ca+Ag)/P ratio of 2.12 ± 0.22 [41].

In general, biocomposites containing CaPO_4 are the main raw material used in elaborating modern technologies for obtaining hybrid biomaterials for medicine. It is desirable to synthesise calcium phosphate composites with polymers to increase their elasticity and bioavailability.

4. Synthesis and Application of Composites of Natural Polymers with HA

In recent years, a huge amount of research has been carried out on composite materials and bioadditives to improve the physicochemical and biological properties of bone tissue, with the aim to prevent and treat osteoporosis. These composite materials include 'ChS-HA', 'Col-HA', 'Col-ChS-HA', 'Col-bioglass', 'ChS-G', 'Col-fibrin', 'HA-protein', and 'fibrin-apatite' [42, 43]. Composites of calcium phosphate, HA, and TKP with a ChS-G complex have been synthesised at molar ratios of 100/0, 90/10, 70/30, 50/50, 30/70, 10/90, and 0/100. These composites contain $\geq 75\%$ calcium phosphate nanoparticles (NPs) and have a porous structure with a porosity of $\approx 95\%$ [44].

The influence of G and HA on the physicochemical properties of their composites has been investigated. By increasing the G amount, the solubility and plasticity of the composite also increased. Mechanically strong and biodegradable G-HA composites have been recommended for use in orthopaedic tissue engineering [26].

In an aqueous solution at 37°C , an organomineral nanocomposite (OMC) of calcium HA, namely $\text{Ca}(\text{OH})_2\text{-H}_3\text{PO}_4\text{-}[\text{C}_6\text{H}_7\text{O}_x(\text{OH})_{3-x}(\text{OCH}_3)_x]_n\text{-H}_2\text{O}$, was synthesised with methylcellulose (MC) $[\text{C}_6\text{H}_7\text{O}_2(\text{OH})_{3-x}(\text{OCH}_3)_x]$. Agglomerates of OMC nanocrystals were obtained by the interaction of HA (150 nm long and 30 nm diameter) with MC (200-500 nm). Improving the properties of the implant on the base synthesised OMC reduces the possible migration of HA into the surrounding tissues owing to the connection between HA NPs and MC. In addition, OMC based on polysaccharides significantly increased the solubility of HA and improved the implantation efficiency [45, 46].

The physicochemical properties and microstructure of composites containing ChS-G and fillers of various chemical compositions of phosphate-calcium materials – HA, TKP, KHA and orthocalcium phosphate (OKP) – have been investigated. The obtained granular materials are elastic with a porosity of 80%, a pore size of $\leq 300\ \mu\text{m}$, and are recommended for use in medicine as porous materials, as well as in the preparation of HA coatings on titanium implants [47].

Researchers have also produced composites consisting of HA-G and HA-G-Ag and have investigated their porosity and bioactivity *in vivo*, and morphology, phase composition, and chemical interactions on the surface. When the HA-G-Ag composite was introduced into a bone defect, it showed high biocompatibility, antibacterial and osteoconductive properties [48].

The interaction between mixtures of CaCl_2 and ChS-polyvinyl alcohol (PVA) (50:50) and their physicochemical properties have been studied. The X-ray spectrum revealed the chemical interaction between ChS-PVA and CaCl_2 and there was an increase in the mechanical strength of the films. Composites are recommended for use in biomedical practice and food packaging [49, 50].

HA and ChS/PVA composites at ratios of 1:1, 1:3, and 3:1 have been obtained. Glutaraldehyde and glycerine have been used as crosslinking agents and plasticisers. The obtained composites were used to stimulate the growth and renewal of bone tissue [51].

Col-HA composites (Ca/P ratio = 1.67) with an adjustable degree of porosity, density, and mechanical properties can be obtained by varying the synthesis conditions. The relationship between the concentration of Ca^{2+} and the properties of composites has been studied in porous structural composites consisting of ChS-Col and mineralised ChS-Col-HA [52-54].



The authors obtained ChS-Col-calcium phosphate composites with porosity $\leq 23\%$, containing 26%-30% Col. To obtain microspheres of ChS calcium phosphate instead of HA, CaCl_2 and NaH_2PO_4 were used at a Ca/P ratio of 2:1 [55].

Composites based on ChS-Col bound with calcium aluminate have been proposed as odontoblast-like material for dental pulp stem cells. The biomembrane was obtained by mixing Col gel with a solution of ChS (2:1) with the subsequent addition of bioactive aluminate calcium cement as a mineral phase. The biological activity of the samples was controlled for 7, 14, and 28 days [56].

PVA-apatite coatings on titanium substrates containing CaCl_2 and NaH_2PO_4 electrolytes were obtained by electrochemical deposition. Depending on the conditions, apatite-polymer coatings containing $\text{CaHPO}_4 \cdot 2\text{H}_2\text{O}$, $\text{Ca}(\text{OH})_2$, amorphous $\text{Ca}_3(\text{PO}_4)_2 \cdot n\text{H}_2\text{O}$, and $\text{HA} - \text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ were recommended for coating the surface of titanium implants [57].

A composite based on bacterial cellulose from *Gluconacetobacter xylinus* (CGX) and HA was synthesised; the morphology of the films was studied using scanning electron microscopy (SEM). HA crystals were arranged monodisperse in CGX microfibrils. The researchers found the following percentages of interactions between the organic and inorganic components of the CGX/HA composite: 50%-56% interfacial electrostatic bonds, 40-46% van der Waals forces, and 2%-7% hydrogen bonds. The presence of electrostatic bonds between calcium phosphate and bacterial cellulose was investigated by modelling. The researchers determined that the energy of interaction of calcium phosphate with bacterial cellulose depended on the chemical structure of HA and the morphology of calcium phosphate [58-60].

Composites of the sodium salt of carboxymethylcellulose (Na-CMC) with HA have been obtained, and their physicochemical properties have been investigated. The researchers determined that carboxyl groups of Na-CMC interact with Ca^{2+} of apatite. Moreover, HA was distributed uniformly in the polymer matrix [61].

In another study, the authors obtained a composite based on ChS-HA-starch and investigated its properties compared with a ChS-HA composite. The ChS-HA-starch composite had hydrogen bonds between the -OH and $-\text{NH}_2$ groups of ChS and the -OH groups of starch and HA [62].

Silk fibroin is used as a good matrix and antimicrobial agent in tissue engineering. Composites suspended with calcium phosphates are biodegradable in living tissues [63].

5. Synthesising ChS-HA Composites and Their Physicochemical Properties

In the literature [64], researchers have reported several methods to synthesise ChS-HA composites. Some methods include forming nanocomposites of the same microstructure synthesised under *in situ* conditions [64, 65], precipitation [66], electrospinning [67-71], hybrid composites [72, 73], solvent evaporation [74], *in situ* chemical methods [75, 76], freezing and lyophilisation [77, 78], combined sintering and freezing, drying methods [79], statistical energy harvesting [80], conventional mixing and heating [81], a biomimetic method [82-84], a low-temperature, wet chemical method [46], a thermal phase separation method [85], a double membrane diffusion method [86], electrochemical deposition and bonding [87-89], electrophoretic deposition [90, 91], mixing of natural HA with ChS [92], and bilateral diffusion [93](Table 1).

Table 1. Methods to prepare chitosan-hydroxyapatite (ChS/HA) composites.

No	Method	Initial components, ChS/HA (Ca/P ratio = 1.67)	Ref.
1	Simple <i>in situ</i> hybridisation: calcium and phosphate salts are obtained at a Ca/P ratio of 1.67 and dissolved together in acetic acid; ChS powder is added under stirring. The mixture precipitates in an alkaline medium at pH 9-10, forming a gel. The final product is then washed and dried	ChS/Ca(NO ₃) ₂ ·4H ₂ O + KH ₂ PO ₄	[72]
2	Casting and solvent evaporation method: the temperature used to evaporate the solvent is defined as the solvent evaporation temperature	ChS/Ca(NO ₃) ₂ ·4H ₂ O + (NH ₄) ₃ PO ₄ ·3H ₂ O	[74]
3	<i>In situ</i> chemical method: hydrogel ChS membranes are immersed in 10 ml of calcium salt solution at 37°C, pH 7.4 for 2 h. Then, it is removed from moisture and dried in a solution of Na ₂ HPO ₄ and then air dried at 37°C	ChS/CaCl ₂ + Na ₂ HPO ₄	[76]
4	HA/ChS bilayer scaffolds: the HA/ChS bilayer scaffolds are fabricated by placing the HA scaffolds into cylindrical silicon moulds and adding 3 wt.% ChS solution. The moulds are frozen and lyophilised up to complete removal of the frozen solvent. Then, HA/ChS bilayer scaffolds are neutralised using a 0.1 M sodium hydroxide solution, frozen, and lyophilised. Finally, the resulting HA/ChS bilayer scaffolds are sterilised using ethylene oxide	ChS + HA (H ₃ PO ₄ /Ca(OH) ₂)	[79]
5	<i>In situ</i> coprecipitation using electrospinning: HA synthesis is carried out in the presence of polymers such as ChS and PVA to produce fibres	ChS/H ₃ PO ₄ + Ca(OH) ₂	[85]
		ChS/Ca(CH ₃ COO) ₂ + (NH ₄) ₂ HPO ₄ /NH ₄ OH	[71]
		KH ₂ PO ₄ /CaCl ₂ /EDTA + ChS/PVA	[69]
6	The biomimetic method is based on obtaining biomaterial that corresponds to bone	ChS/CaCl ₂ + NaH ₂ PO ₄ + phosphate ChS	[82]
		ChS/CaCl ₂ + Na ₂ HPO ₄	[83]
		ChS/Ca(CH ₃ COO) ₂ + NaH ₂ PO ₄ ·H ₂ O and ChS/CaCl ₂ + (NH ₄) ₂ HPO ₄	[84]

No	Method	Initial components, ChS/HA (Ca/P ratio = 1.67)	Ref.
7	Double diffusion method (freezing and lyophilisation): ChS sponges are mineralised in a diffusion chamber consisting of two parts separated by a circular hole in the centre, where ChS is poured. At pH 7.4, buffered solutions of calcium and phosphate salts are obtained with a Ca/P ratio of 1.67. Diffusion through ChS is carried for 4-48 h	ChS/CaCl ₂ + NaH ₂ PO ₄	[86]
		ChS + CaCl ₂ /NaH ₂ PO ₄	[77]
8	Electrophoretic deposition: suspension based on ChS and calcium and phosphate salts at a Ca/P ratio of 1.67 are brought to pH 9-10 and precipitated using various metal electrodes	ChS + HA (Ca(NO ₃) ₂ ·4H ₂ O/ (NH ₄) ₂ HPO ₄)	[88]
		ChS + HA	[81]
		ChS/Ca(NO ₃) ₂ ·4H ₂ O + NaH ₂ PO ₄	[89]
9	Precipitation method (freezing and lyophilisation): a suspension based on ChS and calcium and phosphate salts at a Ca/P ratio of 1.67 is brought to pH 10-11 and precipitated. The samples are lyophilised and dried by freezing	ChS + CaCl ₂ /Na ₂ HPO ₄	[94]
		ChS + CaO = 51.91%; P ₂ O ₅ = 38.25%; MgO = 0.60%; Na ₂ O = 2.84%	[95]
		ChS + CaCl ₂ /NaH ₂ PO ₄	[96]
		ChS/H ₃ PO ₄ + Ca(OH) ₂	[97]
		ChS + nano HA	[78]
		ChS/CaCl ₂ + NaH ₂ PO ₄	[98]
		ChS + HA (H ₃ PO ₄ + Ca(OH) ₂)	[99]
		ChS/CaCl ₂ + KH ₂ PO ₄	[100]
		ChS/Ca(CH ₃ COO) ₂ + NaH ₂ PO ₄	[101]
		ChS/Na ₂ HPO ₄ + CaCl ₂ / Ethanol	[102]
ChS + KHA + (NH ₄) ₂ CO ₃	[42]		
10	One-step coprecipitation: the mixture of ChS and CaCl ₂ is titrated with NaH ₂ PO ₄ solution at a Ca/P ratio of 1.67 and precipitated under alkaline conditions	ChS/CaCl ₂ + NaH ₂ PO ₄	[103]
11	Precipitation method: a suspension consisting of ChS and calcium and phosphate salts at a Ca/P ratio of 1.67 is precipitated at pH 10-11	ChS + HA	[64]
		ChS + HA	[104]
		ChS/Ca(NO ₃) ₂ ·4H ₂ O + (NH ₄) ₃ PO ₄ ·3H ₂ O	[105]
		ChS + nano HA	[106]

No	Method	Initial components, ChS/HA (Ca/P ratio = 1.67)	Ref.
12	Mixed	ChS + Natural HA/CaO/ZnO	[94]
		HA mixing with ChS	[107]
13	Freeze drying technique: ChS/dextran/nano-HA composite scaffold is synthesised via the blending method. Then, the mixture is moulded, frozen to freeze the solvent, and lyophilised in a freeze-dryer at -90°C for 48 h to obtain porous scaffolds	ChS/ Dextran + nHA((Ca(NO ₃) ₂ ×4H ₂ O/ NaH ₂ PO ₄))	[108]

According to the literature, ChS/HA composites have been synthesised from 1 M solutions of CaCl₂ and KH₂PO₄ at a Ca/P ratio of 1.67, instead of HA, and low-molecular-weight ChS with a DD of ≥90%. The researchers obtained granules by precipitating ChS/HA with 5%-7% NaOH; they were then washed with distilled water until reaching a neutral pH, frozen, and dried [100].

ChS/HA and ChS/dicalcium phosphate dihydrate (DCDH) were synthesised by membrane diffusion [94], and their physicochemical properties were investigated. A solution of ChS and CaCl₂ was placed in a semiconductor membrane and immersed in a phosphate solution. After some time, the resulting suspension was freeze-dried. The organic and inorganic contents determined by using thermogravimetric analysis. According to SEM, the composites formed a porous structure. The inorganic content was 35%-45%. X-ray diffraction analysis revealed the formation of HA and DCDH crystals in the polymer matrix.

In a water bath at a Ca/P ratio of 1.67 and 40°C, a mixture of ChS and CaCl₂ was added to Na₂HPO₄ and stirred vigorously. Then, the mixture was precipitated with 1 M NaOH, washed with distilled water, and dried at low pressure. ChS/HA was synthesised at several molar ratios – 30/70, 50/50, 70/30, and 85/15 – and identified by IR spectroscopy, X-ray structural analysis, and thermal analysis. The composites were stable up to 200°C [103].

Maria *et al.* [95] synthesised HA powders heated to 400°C (content: CaO 51.9%; P₂O₅ 38.3%; MgO 0.6%; Na₂O 2.8%) and 700°C (content: CaO 52.3%; P₂O₅ 38.7%; MgO 0.6%; Na₂O 2.1%). HA of the powdered composites interacted with microcrystalline ChS of various molecular weights in mass ratios from 9-1 to 1-9.

Researchers obtained ChS-HA composite fibres by coagulation. For this, they coagulated the ChS-NaH₂PO₄ solution in a special bath filled with Ca²⁺ until homogeneous and then reacted it with NaOH to form a fibrous matrix of HA. The mechanical properties of the fibre depended on the NaH₂PO₄ concentration (0.03 M) in the ChS-NaH₂PO₄ solution [102].

In engineering, several types of polymers and bioceramic materials such as HA composites with various polymers have been elaborated to improve the bioactive, chemical, and mechanical properties of bone tissue. This effort has contributed to improve a number of ceramic properties of HA: internal fragility, structure, and mixing of particles from their location. The authors concluded that these HA hybrid composites are advantageous because the polymers can effectively interact with the tissue surrounding the bone [109].

Silicon-containing apatite prepared from Na₂SiO₃ was obtained and its interaction with ChS was studied. The authors determined that HA [Ca_{10-x}Na_x(PO₄)_{6-x}(CO₃)_x(OH)₂] is



distributed as NPs in the ChS matrix. The effect of the molecular weight of CS on the physicochemical properties and thermal stability of the ChS-HA nanocomposites at 600 and 1000°C was established [84].

ChS/HA composites have also been synthesised for application in bone engineering. The effect of synthesis conditions on the preparation of nanocrystalline structures of apatite has been studied. HA and ChS formed a relatively stable composition in 50/50 ratio. Loss of A-type carbonate ions in HA occurred above 700°C. It was possible to obtain a non-porous composite of A-type by treatment at 1100°C that is closer to the chemical composition of healthy bone tissue [98].

Researchers aimed to determine the optimal composition of ChS/HA composite. To this aim, they synthesised a porous structural composite comprising microcrystalline chitosan (MKChS), HA, and β -tricalcium phosphate (β -TKP) with good adsorption properties. During the investigation, they obtained MKChS- β -TKP-HA composites in various ratios of components and their chemical composition was confirmed on the base of IR spectra. X-ray analysis of calcium phosphate powders has shown their significant amorphous structure at 2θ between 10° and 20° relative to HA, but ChS/ β -TKP exhibited a completely amorphous structure. MKChS/ β -TKP had very high $\text{Ca}^{2+} \text{PO}_4^{3-}$ at a 2:1 ratio [104].

Obtaining ChS-HA nanostructures by the simplest method after morphological analysis of ChS and ChS-HA has allowed researchers to observe irregular, but crosslinked, porous nanocomposites with a more distributed surface area. X-ray and IR spectral analyses confirmed the presence of highly crystalline non-porous HA [110].

6. Preliminary Scheme Regarding the Interaction Between ChS and HA

Researchers have proposed several mechanisms to form apatite and phosphate composites with ChS. These mechanisms depend on the initial components and synthesis conditions. Ca^{2+} play an important role in the interaction between ChS with HA (Figure 3) [62]. Ca^{2+} appear on the surface of HA crystals and firmly hold the structure owing to electrostatic bonds [64, 111, 112]. Consequently, ChS forms crosslinks between NH_2 and Ca^{2+} on HA. The interaction between free NH_2 and protonated amine (NH_3^+) groups of ChS with a solution of acetic acid with HA is characterised as follows:

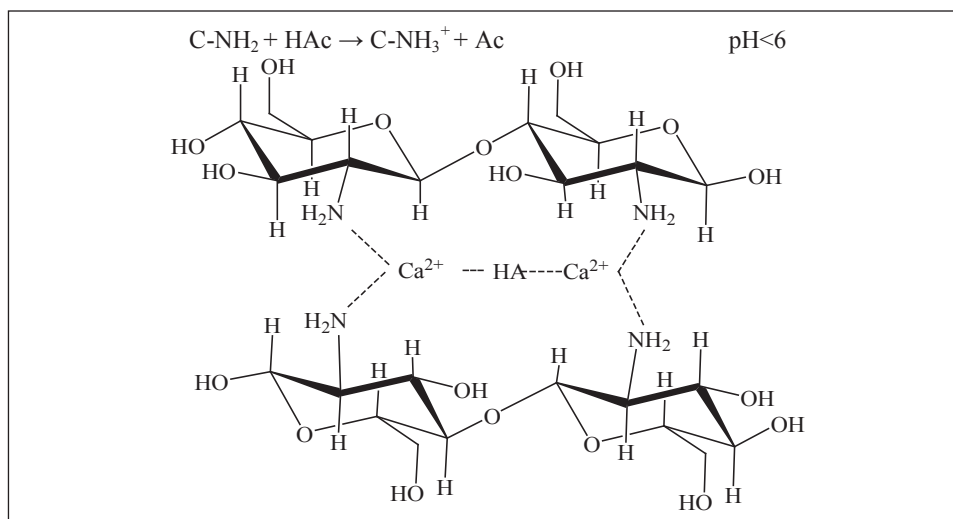


Figure 3. Coordination bonds between the $-\text{NH}_2$ of chitosan and Ca^{2+} of hydroxyapatite (HA) [64, 111, 112].

The presence of Ca^{2+} and PO_4^{3-} in the reaction mixture causes the formation of ChS/HA composites owing to electrostatic interactions between C-NH_3^+ and Ca^{2+} and PO_4^{3-} , and/or C-Ca^{2+} and C-PO_4^{3-} [72, 113]. They also form hydrogen bonds between the $-\text{OH}$ and $-\text{NH}_2$ groups of ChS and the $-\text{OH}$ groups on the HA surface (Figure 4) [74, 108, 110, 113].

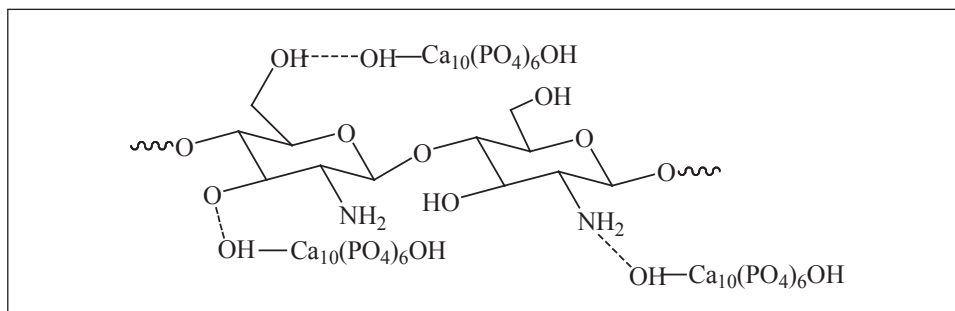


Figure 4. Electrostatic interactions and hydrogen bonds between chitosan and hydroxyapatite [74, 108, 110, 113].

The IR spectrum of ChS shows methylene- CH_2 , amino- NH_2 , methylol- CH_2OH , and aminomethylene- CH_2NH_2 groups. The IR spectra of ChS-HA samples show changes in the amide I and amide II groups in ChS, indicating the interaction between ChS and HA. These interactions can be attributed to hydrogen bonds between $-\text{NH}_2$ and $-\text{OH}$ groups and interactions between $-\text{NH}_2$ and Ca^{2+} . The more the absorption bands of the ChS amino group move in the direction of decreasing wavelengths, the more amine groups of ChS move in the direction of decreasing wavelengths, and the stronger the hydrogen bonds and molecules between these groups [114]. In the investigation of the interaction of the components in the complex of ChS and β -TKP/HA, the authors suggested that Ca^{2+} and PO_4^{3-} interact with amino groups of ChS (Figure 5) [104].

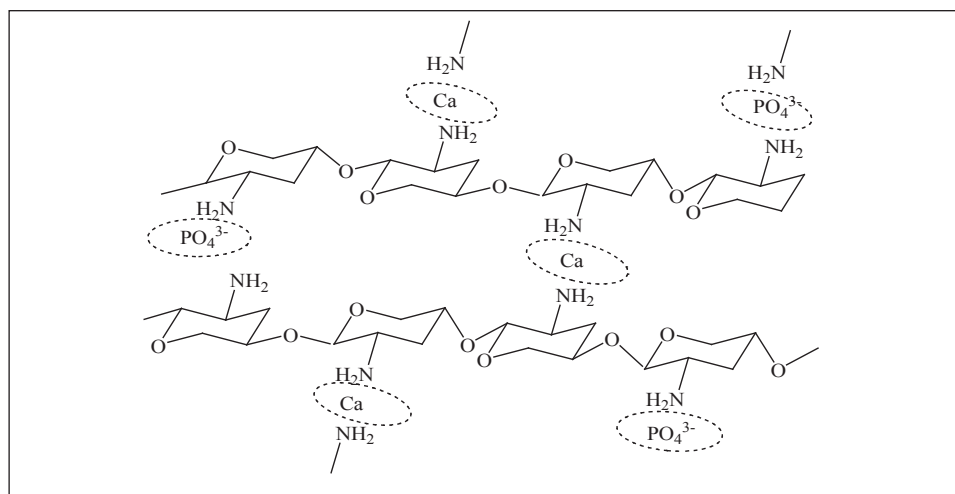


Figure 5. A schematic showing calcium ions (Ca^{2+}) and phosphate ions (PO_4^{3-}) interacting with amino groups of chitosan [104].

Ca^{2+} ions located on the HA surface can bind donor-acceptor (ion-coordination) groups with free $-\text{OH}$ and $-\text{NH}_2$ of ChS, while PO_4^{3-} can bind with partially NH_3^+ groups (Figure 6) [109]. Thus, researchers have established that ChS can interact with HA through donor-acceptor (ion-coordination) bonds, ionic bonds, hydrogen bonds between the $-\text{OH}$ and $-\text{NH}_2$ groups of ChS and $-\text{OH}$ groups on the HA surface, and electrostatic interactions, among others.

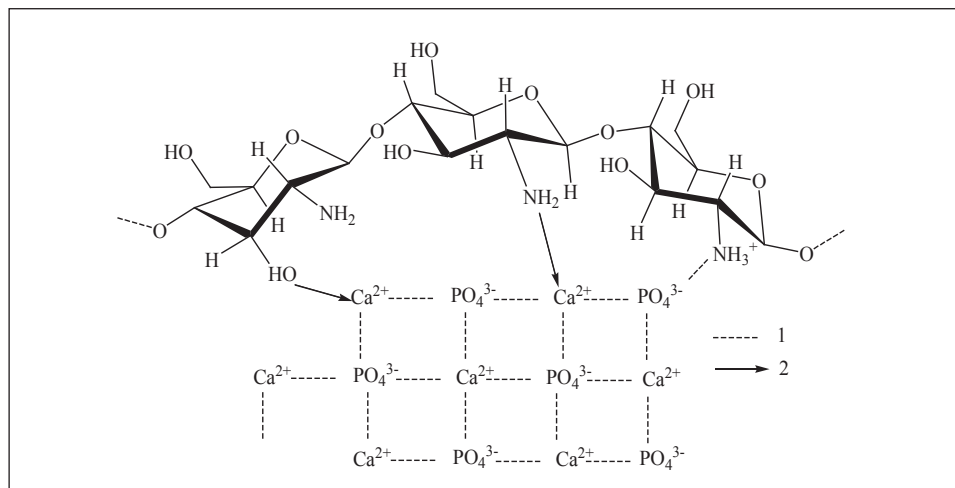


Figure 6. Donor-acceptor and ionic bonds between hydroxyapatite and chitosan [109].

There are various assumptions regarding the mechanism by which ChS interacts with HA. Ca^{2+} interact with amino groups of ChS and have fermi coordination bonds. However, during the interaction of Ca^{2+} with electron donors, functional groups of ChS, there was adsorption of its macromolecules. The adsorption mechanism of metal ions by ChS depends on several factors such as the pH of the solution, the molecular mass of ChS, the DD, particle size, and porosity, among others. Apparently, in solutions containing ChS and HA, Ca^{2+} , PO_4^{3-} , hydrogen phosphate, dihydrogen phosphate ions, and $-\text{NH}_3^+$ have to form electrostatic bonds between the polycation and low molecular mass counterions. In turn, the presence of $-\text{OH}$ groups in the structure of ChS and HA allows the formation of hydrogen bonds. These considerations are in good agreement with published data. Investigations have shown that the interaction between ChS with HA occurs at $\text{pH} < 7$. It is known that in dilute solutions of organic and mineral acids, ChS remains a salt, which causes the interaction between amino groups and metal cations.

In selected conditions of obtaining ChS with Ca^{2+} composites, the pH of the reaction system was always < 7 . The interaction between ChS and HA occurred through electrostatic interactions and hydrogen bonds of ChS ($-\text{NH}_3^+$) and HA ($-\text{HPO}_4^{2-}$ and $-\text{PO}_4^{3-}$) functional groups [115].

Based on experimental and theoretical research methods, the following preliminary scheme for the formation of ChS/HA composites (Figure 7):

1. dissolution of ChS at $\text{pH} < 7$ /protonation of ChS;
2. formation of a ChS/HA suspension;
3. formation of intermediate complexes with the help of electrostatic interactions of components with intensive stirring;
4. growth of an HA crystal under '*in situ*' conditions;
5. neutralisation of the solution and isolation of the target product.

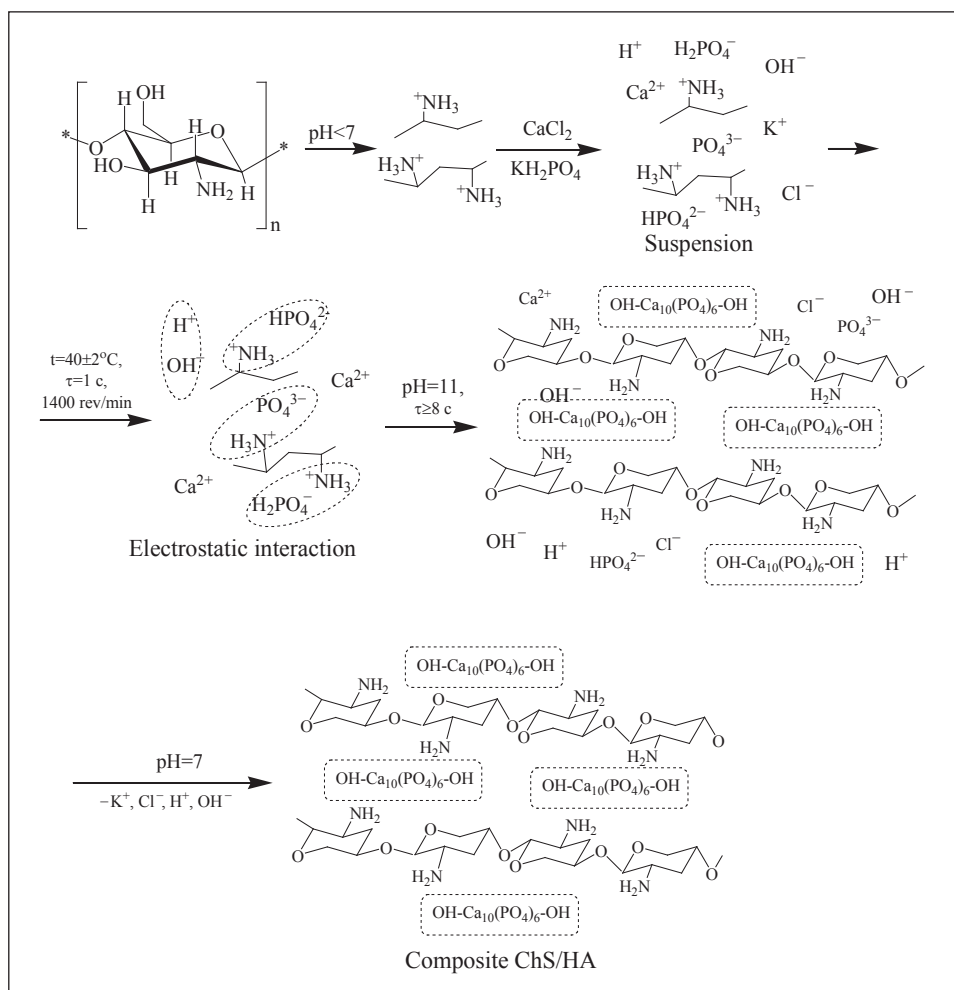


Figure 7. Preliminary scheme for the formation of chitosan and hydroxyapatite (ChS/HA) composites under ‘*in situ*’ conditions [116].

This method makes it possible to obtain ChS/HA composites with a controlled composition and morphology. Based on the literature, the chemical nature of the starting reagents, the order of their addition to the reaction mixture, and the duration of the synthesis are important factors affecting the nature of the interactions and the chemical composition of the final product.

7. The Use of ChS/HA Composites in Medical Practice

Natural bone comprises 69% $\text{Ca}_3(\text{PO}_4)_2$, 21% Col (polymer), 9% water, and 1% other components that form a very complex microstructure, which makes it very difficult to create a structure with similar high mechanical properties [117, 118]. In general, $\text{Ca}_3(\text{PO}_4)_2$ is important for human and mammalian health and because it represents the inorganic part of calcified tissues (bones, teeth, and feathers) and pathological lesions (caused by various diseases associated with calcium and phosphate deficiency) [119, 120]. In addition, $\text{Ca}_3(\text{PO}_4)_2$ is the main source of phosphorus and is used in the production of feed, fertilisers,

detergents, and various phosphorus chemicals. Nanostructured crystalline $\text{Ca}_3(\text{PO}_4)_2$, especially in the form of apatites, play an important role in tissue formation, forming the main inorganic building blocks of skeletal bones and teeth. These complex structures form several tens and hundreds of nanometre crystals of biological apatite. This process is carried out under the strict control of bioorganic matrices (Table 2) [121].

Table 2. Applications of preparations based on chitosan and hydroxyapatite (ChS/HA) composites.

No	Composition of the initial components	Areas of application	Ref.
1	ChS/HA	ChS/HA composite has been investigated in many areas: bone tissue engineering, dentistry, and veterinary medicine	[122-125]
2	ChS/HA (Ca/P ratio of 1.67) 50:50	Bone implants, that is, for the prevention and treatment of osteoporosis	[126]
3	ChS/HA	Chronic periodontitis (infectious and inflammatory dental disease)	[127]
4	ChS/HA and β -TKP/ChS	ChS/HA is used for the treatment of osteoporosis and β -TKP/ChS is used for osteoplasty in dentistry	[128, 129]
5	Porous-structural composites ChS/KHA and ChS/HA	Bone grafting, bone restoration	[70, 130, 131]
6	Composites consisting of ChS, KHA, tetracalcium phosphate, ammonium carbonate, and HA	Used as implants and bone-three-dimensional materials for bone defect engineering	[132]
7	ChS/Ag/HA-poviargol containing composition	Orthopaedic microimplants	[133]
8	ChS/calcium phosphate composite	Bone engineering	[134]
9	ChS/HA/Ag	As an antibacterial (e.g., against <i>Escherichia coli</i> ATCC 25922)	[135]
10	HA/ChS/Ag-poviargol	Orthodontic microimplants	[107]
11	ChS/nano HA	Bone engineering	[80]

No	Composition of the initial components	Areas of application	Ref.
12	Electrospinning fibres of nano-HA/ChS and a composite based on polylactic acid	The treatment of standardised defects of the cranial vault in rats	[136]
13	ChT/HA	Bone defect engineering	[137]
14	3D ChS/HA and HA/ChT composite	Bone grafting in bone engineering	[138, 139]
15	ChS/Col/HA	Bone regeneration	[65, 97, 140]
16	ChS/nano-HA and ChS/starch/nano-HA	For the prevention and treatment of osteoporosis bone regeneration caused by osteoporosis, bone tissue engineering	[78, 105, 141, 142]
17	ChS-coated apatite grafts	In bone tissue engineering	[77]
18	HA/ChS graft	Bone and osteochondral defects	[79]
19	ChS/Col/HA	In bone restoration, transplantation, and treatment of bone recognition defects	[143, 144]
20	Natural HA/ChS	For the treatment of composite bone defects	[92]
21	ChS/HA and ChS/calcium phosphate hydrogels	Promote bone formation and growth in the treatment of bone defects	[145]
22	ChS/HA	Composites have been proposed as biomaterials for restorative dentistry, tissue engineering for alveolar bone and periodontal transplantation for complex dental treatment	[146]
23	ChS/HA and ChS/HA/polycaprolactone	Dental tissue engineering	[147, 148]
24	ChS/HA nanocomposite	Dental fillings	[149]
25	ChS/calcium phosphate C	Composites suitable as a regulatory agent for covering the pulp in dental caries	[150]
26	ChS/HA	To cover the surface of titanium implants	[151]



No	Composition of the initial components	Areas of application	Ref.
27	ChS/HA	ChS/HA composite is intended for enamelling teeth and sealing damaged enamel surfaces	[152, 153]
28	ChS/nano HA	Recommended for use in bone tissue engineering	[154]
29	ChS/HA + polybutyl succinate, bone marrow mesenchymal stem cells, Col, alginate, insulin, etc.	Bone grafting	[155]
30	ChS/HA/carbon nanotubes	Proposed as artificial bones	[156]
31	Porous and block composite materials from montmorillonite nanoparticles and HA from chrysotile, ChT nanofibrils and nanofibers on the base of ChS	Tissue engineering and transplantology	[157]
32	ChS/HA	Bone tissue engineering	[158]
33	KHA/ChS	In medicine (KHA melting in an isotonic solution increase as the ChS concentration increases)	[159]
34	ChS/HA/magnetite	Cell proliferation and bone growth	[160]
35	ChS	Dental surgery	[161]
36	HA/Col	Bone tissue engineering	[162]
37	ChS/HA	Used at internal bone fracture	[163]
38	ChS/Col	Bone tissue engineering, for diseases associated with bone defects	[164]
39	ChS/calcium phosphate	Bone grafting	[165]
40	ChS/tricalcium and monocalcium and dicalcium phosphate	Veterinary practice (osteoporosis and osteomalacia)	[166, 167]

Much work has been done to elaborate drugs based on HA and other calcium phosphates to overcome these problems. Natural and artificial polymers are used to improve the physicochemical properties of these drugs [42]. ChS is specifically relevant among natural polymers owing to its good matrix formation and antibacterial properties. The materials used to fill bone defects must have four main properties: osteoconduction, osteoinduction, osseointegration, and osteogenesis. All these properties are present in ChS. Most

importantly, composites with HA and other calcium phosphates are distinguished by high biological degradation, bioactivity, and antibacterial properties in the correction of bone tissue cell defects [168-171]. NH_3^+ of ChS ensure it readily interacts with DNA, proteins, lipids, charged organic substances or synthetic polymers. These properties of ChS have increased the possibility of using it in composites containing various inorganic and organic compounds in bone tissue engineering [172, 173]. HA/Col nanocomposites are composed of a microstructured porous system resembling bones. However, Col is expensive, can have difficulty binding to bone Col, and does not have suitable flexibility. The introduction of HA into the ChS matrix significantly increases its osteoconductive and mechanical properties [174]. The specific properties of ChS, including its biodegradation, biological flexibility, viscosity, and anti-infective properties, make it an ideal polymer matrix for HA [175].

8. Conclusion

A vast amount of research is being carried out on ChS/HA composites. Each work is unique in its own way and is of fundamental applied interest. However, the available information on the chemical interaction, the influence of the ChS/HA molar ratio, and the molecular weight of ChS on the composition, morphology, and properties of the composite is insufficient. Hence, it is necessary to develop new methods that reduce the crystallisation time of HA in the presence of biocompatible polymers. In this regard, optimisation and improvement of the method for obtaining polymer/HA composites based on *B. mori* ChS and studying the properties and application of these composites are of scientific and practical importance.

9. Abbreviations

AKP	Amorphous calcium phosphates
ChT	Chitin
ChS	Chitosan
Col	Collagen
CMC	Carboxymethylcellulose
CGX	Cellulose <i>Gluconacetobacter xylinus</i>
KHA	Carbonate-hydroxyapatite
DD	Degree of deacetylation
DCDH	Dicalcium phosphate dihydrate
DNA	Deoxyribonucleic acid
EDTA	Ethylenediaminetetraacetic acid
G	Gelatine
HA	Hydroxyapatite
MW	Molecular weight
MC	Methylcellulose
MKChS	Microcrystalline chitosan
NPs	Nanoparticles
OKP	Orthocalcium phosphate
OMC	Organomineral nanocomposite
PVA	Polyvinyl alcohol
PMMA	Polymethyl methacrylate
TKP	Tricalcium phosphate

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